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Space-time Fourier Ptychography for in vivo Quantitative Phase Imaging



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INTRODUCTION

Space-Time Fourier Ptychography (ST-FP)

Challenge: Imaging dynamic, constantly moving biological specimens.

Solution: Combines rapid Fourier Ptychography with space-time motion priors.

Key Features:

Forward Model

- Increased SBP-T: Increases the space-time bandwidth product of the reconstructed complex image sequence while leveraging redundant temporal information to achieve robust reconstruction.
- Applications: Ideal for observing rapid morphological changes in living organisms and reconstructing moving amplitude and phase targets.

Sensor Tube Lens Objective Lens Diving Cells Living Cells Living Cells Living Cells (a) METHODS Forward Warping warp $(o_1, v_1) \approx o_{01}$ Forward Warping warp $(o_1, v_1) \approx o_{01}$ Forward Warping warp $(o_1, v_1) \approx o_{01}$ The Lens Forward Warping warp $(o_1, v_1) \approx o_{01}$ The Lens (b)

deformations between successive frames, a novel reconstruction approach utilizes warping to approximate intermediate frame states. For each time stamp, raw data \mathbf{b}_t is captured under multiplexed illumination. Utilizing motion fields - \mathbf{v}_t and - \mathbf{v}_t , backward and forward warping are applied to estimate \mathbf{b}_{t-1} and \mathbf{b}_{t+1} , respectively. This approach effectively aggregates phase and amplitude information across time, resulting in increased reconstruction accuracy and resolution. This method aligns each captured raw frame with its temporal stamp, allowing for the reconstruction of objects even with significant motion, as opposed to the traditional scheme that requires negligible object movement.

(b) (e) Sensor A Optical System (c) (f) Multiplexed Imaging Imaging (h)

Schematic of Fourier Ptychography (FP) with multiplexed illumination.

(a) A single low-resolution (LR) image captured under a specific LED pattern, is indicative of the spatial frequency information of the object. (b)-(d) Resultant frequency domain representations, showing the spatial frequency shifts induced by different illumination angles. (e)-(g) Sub-images corresponding to different spatial frequency regions obtained under varied LED illuminations. (h) The imaging system schematic illustrates the pathway from multiplexed illumination to the sensor.

ST-FP Framework

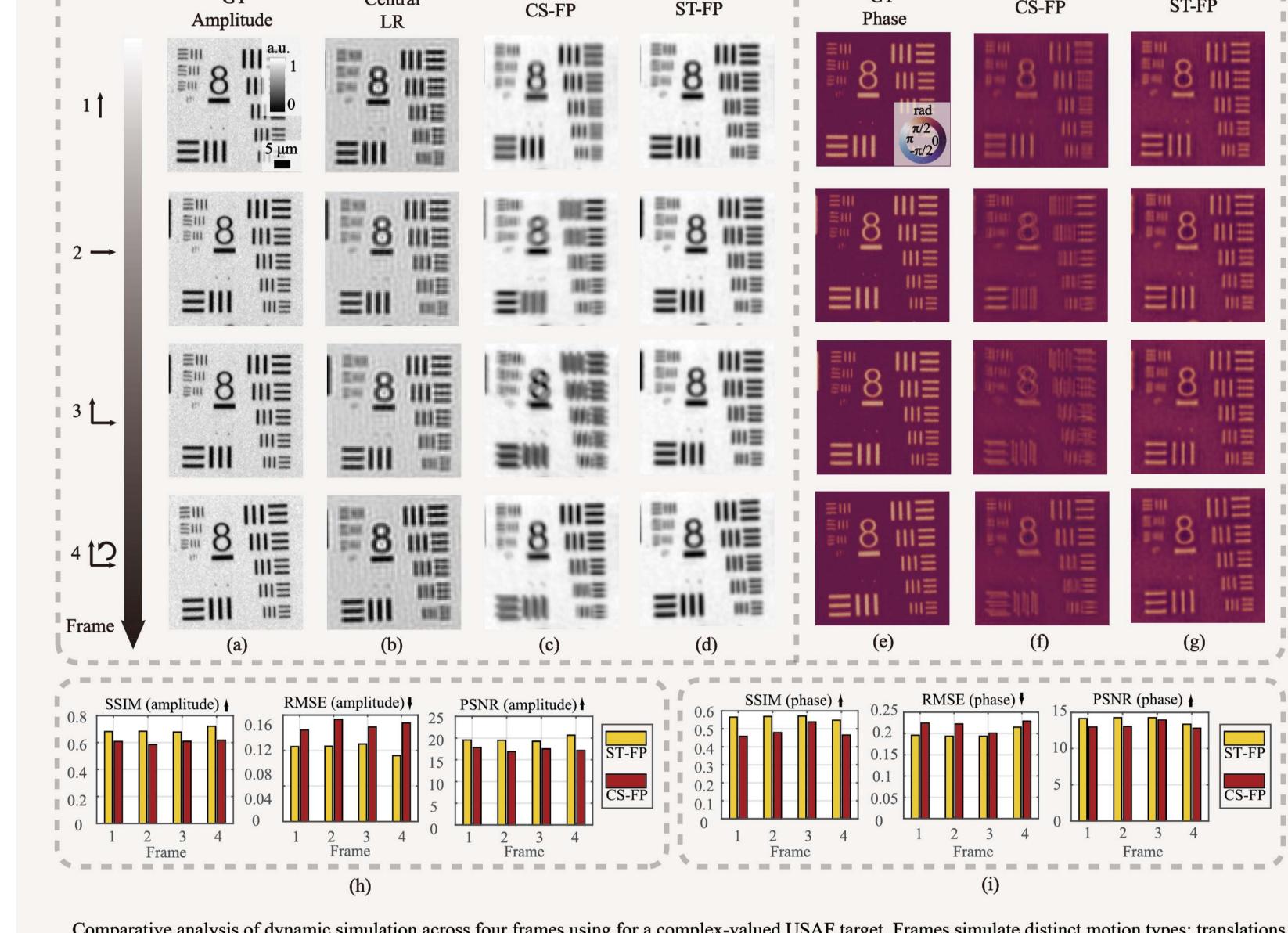
 $\min_{\mathbf{o}_{t}, \mathbf{v}_{t} \}_{t}} \sum_{t=1}^{1} \left\| \mathcal{A}_{t}(\mathbf{o}_{t}) - \mathbf{b}_{t} \right\|_{2}^{2} + \alpha \sum_{t=1}^{1-1} \left\| \mathbf{D}_{t} \right| \mathbf{o}_{t} + \mathbf{D}_{s} \left| \mathbf{o}_{t} \right| \cdot \mathbf{v}_{t} \right\|_{2}^{2} \\
+ \gamma \left(\sum_{t=1}^{T-1} \left\| \mathcal{A}_{t+1}(\operatorname{warp}(\mathbf{o}_{t}, \mathbf{v}_{t})) - \mathbf{b}_{t+1} \right\|_{2}^{2} + \sum_{t=2}^{T} \left\| \mathcal{A}_{t-1}(\operatorname{warp}(\mathbf{o}_{t}, -\mathbf{v}_{t-1})) - \mathbf{b}_{t-1} \right\|_{2}^{2} \right) \\
+ \beta \sum_{t=1}^{T-1} \left(\left\| \mathbf{D}_{s} \mathbf{v}_{t,x} \right\|_{\mathbf{H}_{\mu_{1}}} + \left\| \mathbf{D}_{s} \mathbf{v}_{t,y} \right\|_{\mathbf{H}_{\mu_{1}}} \right) + \delta_{1} \sum_{t=1}^{T} \left\| \mathbf{D}_{s} \mathbf{o}_{t} \right\|_{\mathbf{H}_{\mu_{2}}} + \delta_{2} \sum_{t=1}^{T-1} \left\| \mathbf{D}_{t} \mathbf{o}_{t} \right\|_{\mathbf{H}_{\mu_{3}}}$

The first term is the data fidelity term for the individual measurements. $\mathcal{R}(\cdot)$ is the forward multiplexing function for frame t, $\mathbf{0}$, is the (complex-valued and \emph{moving}) object at time t, and \mathbf{b} , represents the observed measurement. The second term is the optical flow term that jointly estimates the velocity / motion of the object. \mathbf{D}_i and \mathbf{D}_s are the temporal and spatial discrete gradient operators, implemented as one-sided divided differences. \mathbf{V}_i is the velocity field estimated for the motion from the amplitude image $|\mathbf{0}_i|$ to amplitude image $|\mathbf{0}_{i+1}|$. The next line incorporates the warp-and-project method, in which the partial reconstruction of the object at time t is warped

forward (and backward) in time, undergoes the image formation model \mathcal{A}_{H} at that time (project), the result of which is compared to the measurement \mathbf{b}_{H} obtained for that time.

The final line has several smoothness regularizers for both the motion field (in space) and the object (in space and time). For these smoothness terms we utilize the Huber penalty function $\|\cdot\|_{H}$, which provides a tradeoff between the 11 and 12 norms. $\gamma, \alpha, \beta, \delta_1$ and δ_2 are weights of the different terms.

Simulation Results

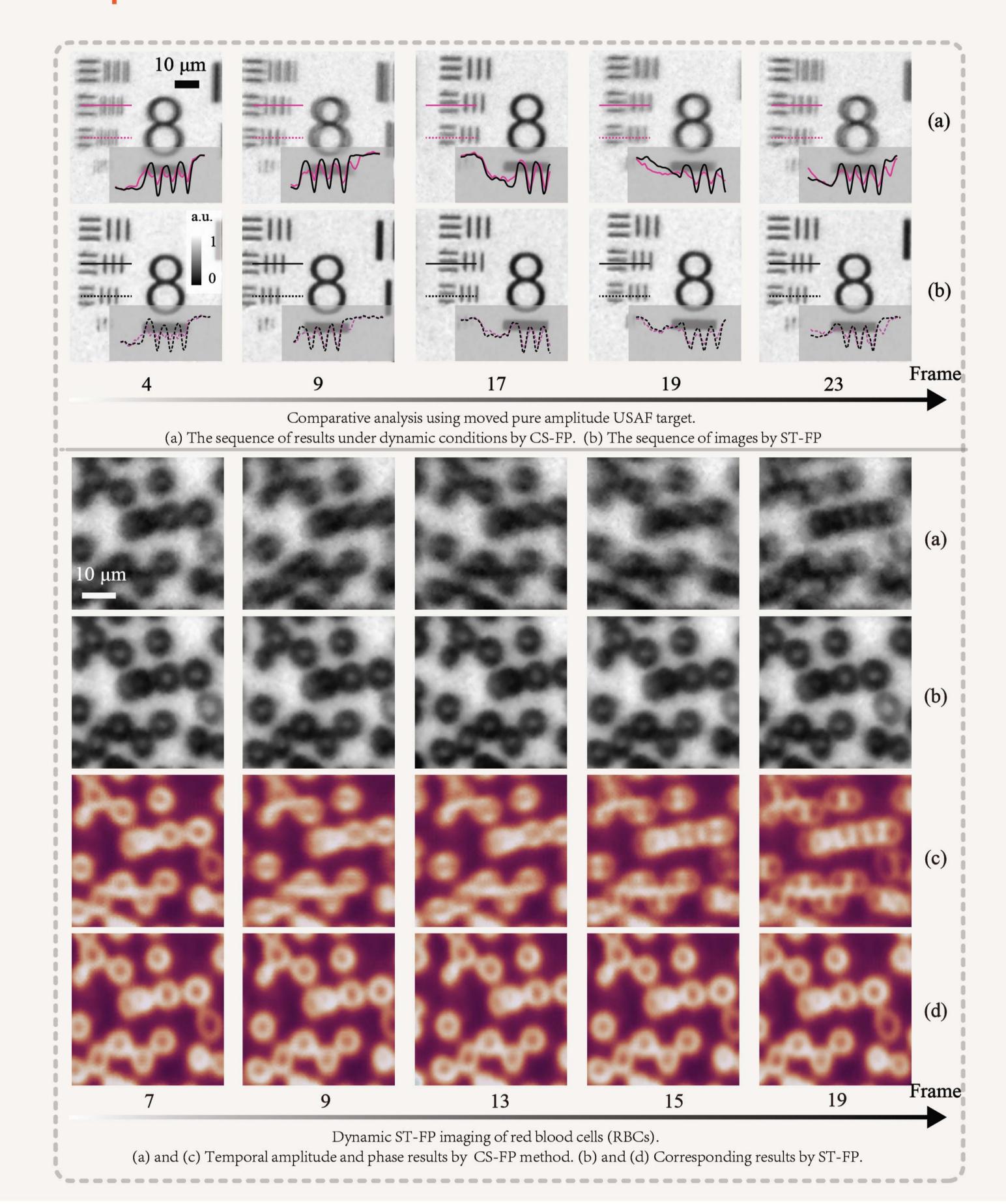


along the y-axis, x-axis, combined x-y axes, and a composite translation-rotation motion. (a) Ground truth (GT) for amplitude. (b) LR sub-image under central FP system illumination. (c-d) Amplitude reconstruction for CS-FP and proposed ST-FP. (e) GT for phase. (f) and (g) are phase results of CS-FP and ours. (h) and (i) Comparison of amplitude and phase reconstruction quality against the GT, using SSIM, RMSE, and PSNR metrics for both CS-FP and ST

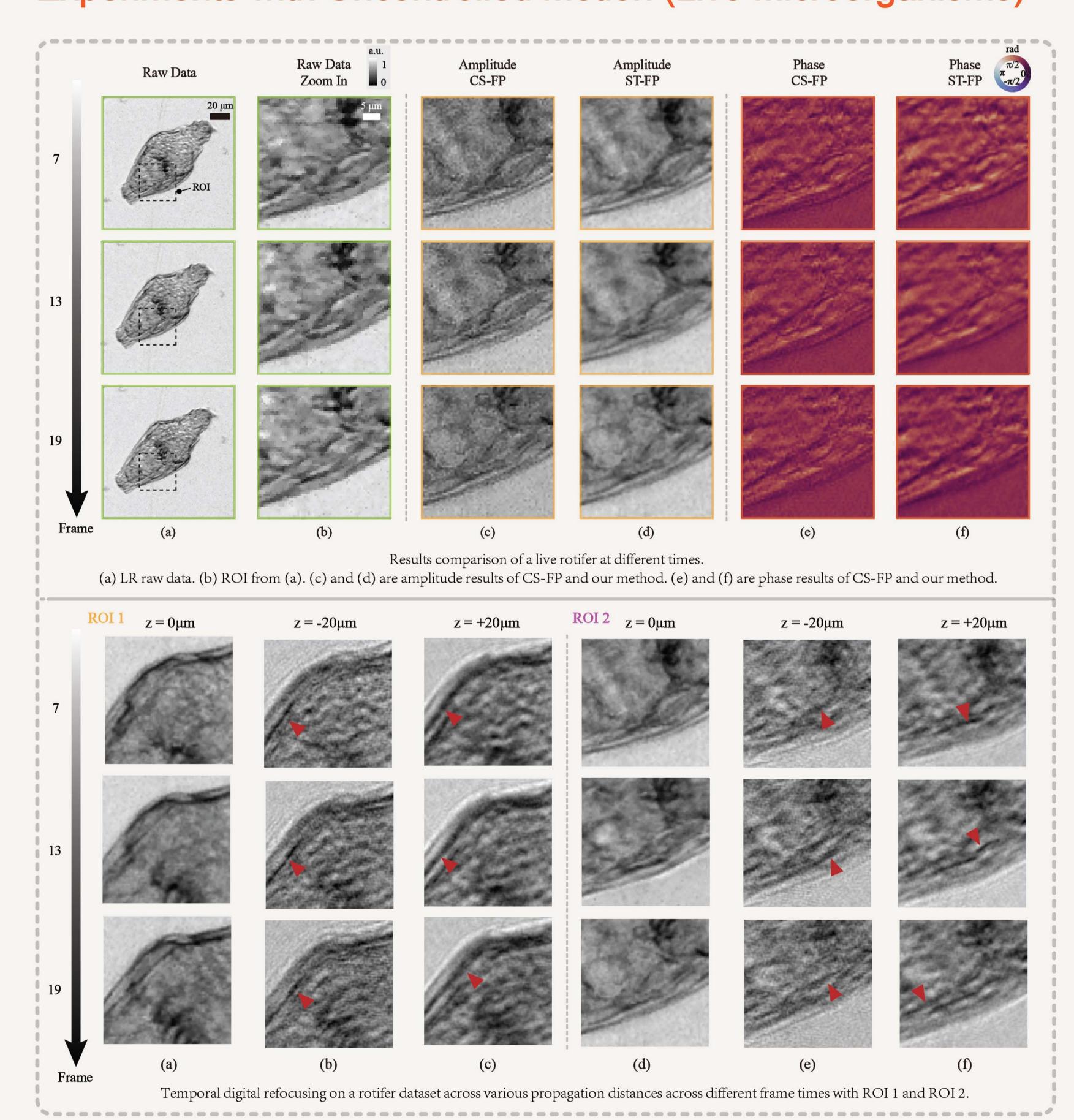
			iits (USA	F target)	
SS.	IM↑	RM	ISE↓	PSN	JR ↑
Frame ST-FP	CS-FP	ST-FP	CS-FP	ST-FP	CS-FP
1 0.6822	0.6087	0.1056	0.1288	19.5294	17.8000
2 0.6838	0.5837	0.1061	0.1439	19.4861	16.8406
3 0.6778	0.6090	0.1092	0.1333	19.2349	17.5047
4 0.7211	0.6172	0.0928	0.1390	20.6487	17.1415

RESULTS

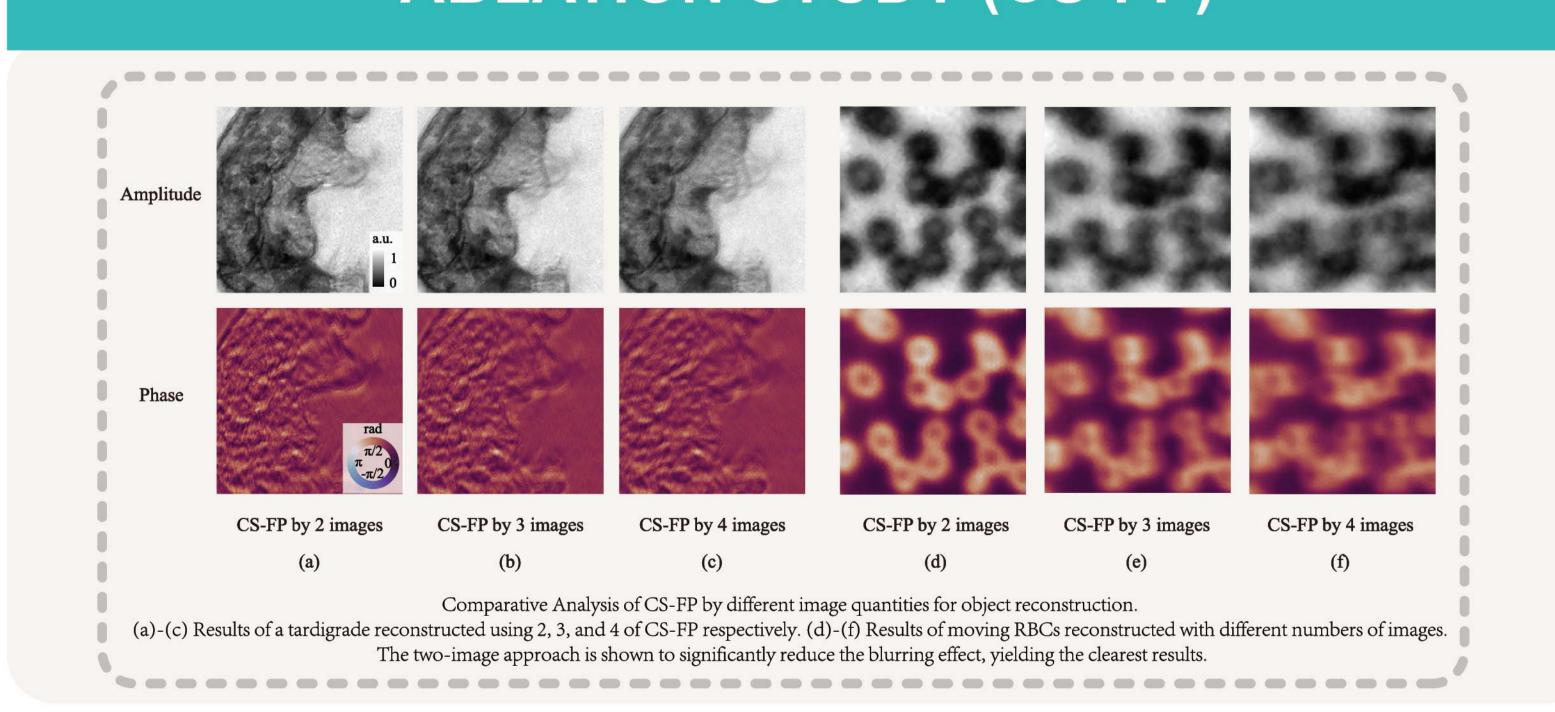
Experiments with Controlled Motion



Experiments with Uncontrolled Motion (Live Microorganisms)



ABLATION STUDY (CS-FP)



REFERENCES

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